Distinct intracellular Ca^{2+} dynamics regulate apical constriction and differentially contribute to neural tube closure

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KEY WORDS
Actomyosin, apical constriction, calcium ion, epithelial remodeling, neural tube closure
ABSTRACT

Early in the development of the central nervous system, progenitor cells undergo a shape change, called apical constriction, that triggers the neural plate to form a tubular structure. How apical constriction in the neural plate is controlled, and contributes to tissue morphogenesis, are not fully understood. In this study, we show that intracellular calcium ions (Ca$^{2+}$) are required for *Xenopus* neural tube formation, and that there are two types of Ca$^{2+}$-concentration changes, a single-cell and a multicellular wave-like fluctuation, in the developing neural plate. Quantitative imaging analyses revealed that transient increases in Ca$^{2+}$ concentration induced cortical F-actin remodeling, apical constriction, and accelerations of the closing movement of the neural plate. We also show that extracellular ATP and N-cadherin participate in the Ca$^{2+}$-induced apical constriction. Furthermore, our mathematical model suggests that the effect of Ca$^{2+}$ fluctuations on tissue morphogenesis was independent of its frequency, and fluctuations affecting individual cells were more efficient than those at the multicellular level. We propose that distinct Ca$^{2+}$ signaling patterns differentially modulate apical constriction for efficient epithelial folding and this mechanism has broad physiological outcomes.

SUMMARY STATEMENT

Rapid cell shape changes mediated by the two spatiotemporal patterns of Ca$^{2+}$ fluctuations, extracellular ATP, and N-cadherin control epithelial folding during central nervous system development.
INTRODUCTION

The construction of multicellular biological system requires substantial tissue movement based on the collective motility of single cells. Problems such as congenital malformations, breakdown of homeostasis, and cancer can arise when the mechanisms that guide the concerted movement of single cells are dysfunctional (Guillot and Lecuit, 2013). In vertebrates, the central nervous system (CNS) is established during early embryogenesis by the collective closing movement of an epithelial sheet of neural progenitor cells in a process called neural tube closure (NTC), and NTC failure causes a common human birth defect (Copp et al., 2003; Suzuki et al., 2012). During NTC, neuroepithelial cells on the dorsal side contract and stabilize their apical sides to change from a columnar to a wedge shape. As a common strategy for folding an epithelial sheet, this cellular morphogenesis called apical constriction (AC) generates physical force to bend the neural plate (NP) inward (Martin and Goldstein, 2014; Sawyer et al., 2010; Suzuki et al., 2012). The lateral edges of the bending neural plate lift above the dorsal surface, eventually come together along the dorsal midline, and fuse to form the neural tube.

AC involves the accumulation of actin filaments (F-actin) at the apical side, where non-muscle myosin II generates contractile force. Thus, AC is thought to be controlled by a coordinated action of cytoskeletal networks, cell-cell adhesions, and their regulators (Martin and Goldstein, 2014; Sawyer et al., 2010; Suzuki et al., 2012). However, how AC in the individual cell is controlled collectively within the tissue, and how AC contributes to tissue remodeling, are not fully understood. Recent studies have revealed that the AC in Drosophila and C. elegans epithelial invaginations is highly dynamic and is governed by oscillations of the apical actomyosin network, in which cell contraction is followed by stabilization (Martin and Goldstein, 2014; Mason et al., 2013; Sawyer et al., 2010). Hence, we hypothesized that the signaling pathway that induces rapid cellular behaviors controls AC in NTC.

In this study, we examined the roles of intracellular calcium ion (Ca\(^{2+}\)) signaling in NTC. Generally, the intracellular Ca\(^{2+}\) concentration is maintained at a low level under basal conditions, and is transiently increased by Ca\(^{2+}\) influx through membrane-localized Ca\(^{2+}\) channels or release from the endoplasmic reticulum via channels such as the inositol triphosphate receptor (IP\(_3\)R) (Clapham, 2007). Ca\(^{2+}\) binds and activates its target proteins that control diverse biological phenomena, such as cell proliferation, muscle contraction, gene expression, and cellular movement (Clapham, 2007; Markova and Lenne, 2012). Inhibiting Ca\(^{2+}\) influx causes NTC to fail (Lee and Nagele, 1986; Smedley and Stanisstreet, 1986), while inducing an increase in intracellular Ca\(^{2+}\) promotes folding morphogenesis of the NP (Ferreira
and Hilfer, 1993; Moran and Rice, 1976). Since these effects at the tissue level are accompanied by changes in cell shape (Ferreira and Hilfer, 1993), intracellular Ca\textsuperscript{2+} signaling has been proposed to regulate AC, although the detailed molecular mechanism is unclear.
RESULTS

Physiological significance of intracellular Ca\textsuperscript{2+} in neural tube closure.

We first examined the role of intracellular Ca\textsuperscript{2+} signaling in NTC in the African clawed frog, *Xenopus laevis* (Fig. S1) by pharmacological treatments. Perturbing the Ca\textsuperscript{2+} influx with 2-aminoethoxydiphenyl borate (2APB, which blocks IP\textsubscript{3}R and other membrane-localized Ca\textsuperscript{2+} channels) or with nifedipine (which blocks voltage-dependent Ca\textsuperscript{2+} channels) inhibited NTC (Fig. 1A). We confirmed these results by measuring the width of NP with the pan-neural marker Sox2 (Fig. 1B). Phalloidin staining revealed that AC in NP cells was inhibited, thus delaying folding morphogenesis of the NP (Fig. 1C,D). Since these inhibitors did not change the expression patterns of marker genes (Fig. 1E), it is suggested that Ca\textsuperscript{2+} signaling regulates AC during NTC independently of neural development.

Live-imaging analyses of Ca\textsuperscript{2+} fluctuation.

In a number of organisms including *Xenopus*, active changes of intracellular Ca\textsuperscript{2+} concentration have been observed during development (Hunter et al., 2014; Leclerc et al., 2000; Markova and Lenne, 2012; Shindo et al., 2010; Wallingford et al., 2001). Therefore, we hypothesized that Ca\textsuperscript{2+} signaling is spatially and temporally correlated with cellular morphogenesis. We investigated the patterns of intracellular Ca\textsuperscript{2+} concentration changes during NTC using live cell-imaging analyses with transiently-expressed genetically encoded Ca\textsuperscript{2+} indicators for optical imaging (GECOs) (Fig. S2A) (Zhao et al., 2011). The intensity of R-GECO1.0 fluorescence fluctuated actively throughout the NP at both single-cell and whole-tissue levels (Fig. 2, Movie 1). In this study, we defined a single increase and the following decrease in GECO fluorescence intensity as a Ca\textsuperscript{2+} “transient.” We observed two spatial patterns of Ca\textsuperscript{2+} transients, one that occurred at the single-cell level and lasted less than 40 seconds (Fig. 2A,C), and the other that originated from one or a few cells and propagated radially, wave-like, across neighboring cells until anywhere from several cells to hundreds of cells were involved (Fig. 2B, Movie 2). These multicellular Ca\textsuperscript{2+} fluctuations lasted up to 100 seconds (Fig. 2C). The fold changes in fluorescence intensity were larger at the multicellular level than that at the single-cell level (Fig. 2C). The multicellular waves spread at a speed of 3.3 ± 0.94 µm/s (mean ± s.d.), and larger waves spread at higher speeds (Pearson's $r = 0.499$, $P = 0.0213$, Fig. 2D), suggesting a relationship between the wave propagation and the spatial strength of the Ca\textsuperscript{2+} signaling contributes to diverse patterns of the Ca\textsuperscript{2+} fluctuation.
Quantitative analyses of the Ca\textsuperscript{2+} fluctuation.

To characterize the spatial and temporal patterns of these Ca\textsuperscript{2+} fluctuations more precisely, we conducted quantitative image analyses based on ratiometric imaging (Fig. S2B, Materials and Methods). After extracting and visualizing the Ca\textsuperscript{2+} fluctuation profiles, we confirmed that most of the Ca\textsuperscript{2+} transients occurred in the NP rather than in the non-neural ectoderm (Christodoulou and Skourides, 2015), which is lateral to the NP and does not undergo folding morphogenesis (Fig. 3A). We quantified the number of Ca\textsuperscript{2+} transients as a function of time, and found that the number of single-cell transients particularly increased in the last 100 minutes before NTC completed (Fig. 3B,C, Fig. S3A). Therefore, we divided the NTC process into an early and a late phase (Fig. 3B). The number of multicellular transients was one order of magnitude smaller than that of single-cell transients throughout the NTC process, and stayed the same level throughout both the early and late phases (Fig. 3D). Taken together, these results suggested that single-cell Ca\textsuperscript{2+} transients were more frequent in the late phase than the early phase, whereas the spatial scale (the propagative property) of the Ca\textsuperscript{2+} transients was larger in the early phase than in the late phase. The technical limitations of our method did not allow us to segment individual cell outlines, so we could not compare the total number of cells contributing to the Ca\textsuperscript{2+} transients. Therefore, we determined the total area of each type of transient, and confirmed that the ratio of the multicellular transients to the single-cell transients decreased from 0.55 to 0.18 in the late phase of NTC (Fig. 3E). These results suggested that the effect of Ca\textsuperscript{2+} fluctuations on NTC was derived from both single-cell and multicellular transients in the early phase, but mostly from single-cell transients in the late phase.

Ca\textsuperscript{2+} fluctuation precedes neural tube closure

In our observations, the multicellular wave-like Ca\textsuperscript{2+} propagations were associated with a slight deformation of the neural plate tissue (Movies 1,2). Together with the observations that perturbation of Ca\textsuperscript{2+} influx inhibited NTC, it is suggested that intracellular Ca\textsuperscript{2+} signaling is essential for the movements that close the neural tube. We compared the temporal pattern of NTC movements with the total intensity values of R-GECO1.0 at tissue level. As expected, peaks in the R-GECO1.0 temporal profile overlapped with peaks in the speed of the closing movements, both in the early and late phase (Fig. 3F). Cross-correlation analyses revealed a maximum correlation when the R-GECO1.0 value was shifted 20 seconds later in time (Fig. 3G). Thus, the Ca\textsuperscript{2+} fluctuation slightly and consistently preceded the tissue movements to close the neural tube.
Regulatory mechanisms upstream of the Ca\(^{2+}\) fluctuation.

We examined the effect of the pharmacological treatment on the Ca\(^{2+}\) fluctuation. 2APB suppressed both the single-cell and multicellular transients in the early phase, whereas nifedipine did not clearly exhibit suppression effects on the multicellular transients (Fig. 3A-D, Fig. S3A). These results suggested that the IP\(_3\)R pathway regulates both types of Ca\(^{2+}\) transients, whereas the voltage-dependent Ca\(^{2+}\) channel preferentially regulates Ca\(^{2+}\) transients at the single-cell level. Cross-correlation analyses revealed that 2APB completely abolished the temporal correlation between Ca\(^{2+}\) fluctuations and the NP’s movements toward closing the neural tube compared with nifedipine (Fig. 3G). This difference might be due to residual multicellular transients in the nifedipine-treated embryo that induced a transient acceleration in the closing movement of the NP (Fig. 3D). Treatment with 2APB or nifedipine did not affect the basal intracellular Ca\(^{2+}\) level as estimated by the ultrasensitive Ca\(^{2+}\) indicator yellow Cameleon-Nano (YC-Nano) (Horikawa et al., 2010) (Fig. S3B). This result suggests that, at the concentrations used, these inhibitors selectively affected the active Ca\(^{2+}\) fluctuations, and therefore, that the active Ca\(^{2+}\) signaling is required for NTC.

During *Xenopus* gastrulation, a purinergic receptor (Corriden and Insel, 2010; Schwiebert and Zsembery, 2003) for extracellular ATP (eATP) is required for frequent Ca\(^{2+}\) elevations (Shindo et al., 2010; Wallingford et al., 2001), and early ectodermal cells respond to eATP causing transient contractions of their apical side (Kim et al., 2014). To examine the possibility that eATP is involved in Ca\(^{2+}\) fluctuations in the NP, we exhausted the eATP by overexpressing *Xenopus* ectonucleoside triphosphate diphosphohydrolase 1 (E-NTPDase1) (Masse et al., 2007). E-NTPDase1 decreased the frequency of both single-cell and multicellular Ca\(^{2+}\) transients compared to an enzymatically inactive variant of E-NTPDase1 (ΔACR) (Fig. 4A-C, Fig. S3C, Movie 3). Moreover, overexpressing E-NTPDase1 abolished the temporal correlation between Ca\(^{2+}\) fluctuations and the closing movements of the NP, as seen with the 2APB treatment (Fig. 4D). We further examined eATP’s involvement in Ca\(^{2+}\) fluctuations using the fluorescence resonance energy transfer (FRET)-based ATP indicator ATeam3.10 (Imamura et al., 2009). We found that extracellularly expressed ATeam3.10 increased the ratio of yellow/cyan fluorescence on the cell membrane compared with a mutant form of ATeam3.10 that is unable to bind ATP (RK mutant) (Fig. 4E,F). Co-expressing E-NTPDase1 suppressed this increase in the ratio of yellow/cyan fluorescence, but co-expressing the ΔACR variant did not (Fig. 4E,F). Taken together, these data suggest that...
eATP exists in the NP and regulates the Ca\(^{2+}\) fluctuations.

**Ca\(^{2+}\) transients induce cortical F-actin remodeling and apical constriction.**

Ca\(^{2+}\) fluctuations in the embryo regulate various cellular behaviors such as the cell flattening (Markova and Lenne, 2012), cell intercalation and polarization (Shindo et al., 2010; Wallingford et al., 2001), and cell contraction (Hunter et al., 2014). In addition, during wound healing in the developing epidermis, multicellular, wave-like Ca\(^{2+}\) transients accelerate the closure process through cell-shape changes (Antunes et al., 2013; Herrgen et al., 2014), suggesting that Ca\(^{2+}\)-mediated cellular mechanisms underlie tissue development and homeostasis through epithelial remodeling. We investigated the relationship between Ca\(^{2+}\) fluctuations and NTC at the cellular level by simultaneously imaging R-GECO1.0 and the F-actin marker Lifeact-EGFP, which highlights the cell periphery (Riedl et al., 2008). We found that immediately after a Ca\(^{2+}\) transient, mesh-like F-actin structures developed in the center of the cell and were maintained for several minutes even after the Ca\(^{2+}\) dropped back to basal levels within a few tens of seconds (Fig. 5A, +60s to +160s, and 5B, Movie 4). Furthermore, the area of the apical side of the NP cells decreased rapidly and then stabilized within a minute after a Ca\(^{2+}\) transient (Fig. 5A,B, Movie 4). Cross-correlation analyses among the R-GECO1.0 values, medial F-actin, and cell-area dynamics revealed that the maximum correlation with the F-actin signals was obtained at time lag 0, whereas with the cell-area dynamics it occurred when the R-GECO1.0 value was shifted later in time (Fig. 5C), which corresponded with tissue-level analysis (Fig. 3G). These suggest that the rapid activation and prolonged F-actin remodeling induced by Ca\(^{2+}\) may be the mechanism of AC and NTC by which relaxation to the original state (i.e., before Ca\(^{2+}\) transients occurred) is suppressed. We could not determine whether the Ca\(^{2+}\)-induced F-actin remodeling was due to overall polymerization or to the relocalization of F-actin to the apical side; both processes are implicated in the rapid cell contractions during *Drosophila* mesodermal invagination (Mason et al., 2013). In addition, it is also possible that non-muscle myosin II is activated by Ca\(^{2+}\) transients through known pathways such as calmodulin-dependent kinase (CaMKII)-mediated RhoA (Murakoshi et al., 2011) and myosin light chain kinase (MLCK) activation (Vicente-Manzanares et al., 2009).

We addressed the causal relationship between the Ca\(^{2+}\) transient and AC by using NPE-caged IP\(_3\) and DMNPE-caged ATP to experimentally induce Ca\(^{2+}\) transients. Brief ultraviolet (UV) illumination applied to an embryo injected with NPE-caged IP\(_3\) induced a localized Ca\(^{2+}\) transient (Movie 5), followed by a decrease in the apical-side area of the
UV-illuminated NP cells compared with that of unilluminated cells (Fig. 5D). Furthermore, by uncaging DMNPE-caged ATP applied to the ringer solution, we induced an intense multicellular Ca\(^{2+}\) propagation wave followed by the shrinkage of NP cells at the tissue level (Fig. 5E, Movies 6,7). Since F-actin in the medial region is linked to the junctional cadherin complexes during AC (Martin and Goldstein, 2014; Mason et al., 2013; Sawyer et al., 2010), we focused on N-cadherin, which is required for F-actin assembly in the NP (Morita et al., 2010; Nandadasa et al., 2009). We found that blocking the function of N-cadherin in DMNPE-caged ATP-stimulated NP cells inhibited the decrease in apical area (Fig. 5E, Movies 8,9). These data suggest that the Ca\(^{2+}\) transients induce AC in NP cells, and that N-cadherin plays a role in the Ca\(^{2+}\)-induced AC.

**Mathematical analysis of neural tube closure based on pulsed apical contraction.**

Our experimental results raise the possibility that the Ca\(^{2+}\) fluctuations function in decreasing the total apical area of the NP. It is possible that Ca\(^{2+}\) fluctuations modulate cellular properties or mechanical processes. Indeed, we have demonstrated that Ca\(^{2+}\) fluctuations appeared to regulate the localization of F-actin, which is involved in both cell properties and mechanical processes. There are two types of transient Ca\(^{2+}\) fluctuations: those that occur at the single-cell level, and those that occur at the multicellular level. In order to evaluate differences in the effect and function of each type of Ca\(^{2+}\) fluctuation at the cellular level on tissue deformation, we constructed a multi-cell-based mechanical model, in which the Ca\(^{2+}\) fluctuations modulate a cellular mechanical parameter of a simplified epithelial tissue (Fig. 6A, Supplementary Materials and Methods). Our model is based on the vertex model, which is a well-known mathematical framework used to describe multicellular tissue dynamics (Farhadifar et al., 2007; Nagai and Honda, 2001; Okuda et al., 2013; Rauzi et al., 2008). To examine how the transient and patterned modulation of mechanical processes or properties in the cell results in the persistent shrinkage of an epithelial sheet, we introduced two components to our model. The first is the mechanical effect of the Ca\(^{2+}\) transient as a modification of the line tension of the cellular edges over a short time period (Fig 6B), which is expected to decrease the cell surface area (see Supplementary Materials and Methods for definition). The second is the constrictive nature of apical cell surface with ratchet (Fig. 6C,D): the cells’ natural surface area and the cells’ natural perimeter are permitted to decrease but not to increase (see Supplementary Materials and Methods for definition). In our model, by regulating the spatial
and temporal pattern of the modification of the line tensions, the effect of the Ca\(^{2+}\) transient at the single-cell and the multicellular levels can be simulated. Furthermore, the regulations of the cells’ natural surface area and the cells’ natural perimeter enabled us to introduce a ratchet-like mechanism (Martin and Goldstein, 2014; Mason et al., 2013; Sawyer et al., 2010) that has not been previously introduced (Spahn and Reuter, 2013).

Using this model, we first examined the combined effect of the Ca\(^{2+}\) transient (pulse) and the constrictive nature of apical cell surface (Acn) on the modeled epithelial tissue. Without either of these components and with the pulse component alone, the tissue size rarely changed at the end of the simulation time (Fig. 7A,B). Interestingly, adding the Acn component caused the modeled tissue to gradually decrease in size, and the combination of pulse and Acn components accelerated such decreasing behavior (Fig. 7A,B, Movie 10). At the single-cell level, transiently increased potential energies of apical surface area and perimeter, which were induced by modification of line tension during single pulse, led to contraction of apical surface area and perimeter, respectively (Fig. 7C and Fig. S4). When the Acn component existed, those contractions further resulted in the irreversible decrease of the natural surface area and the natural perimeter (Fig. 7C and Fig. S4). Interestingly, after the contractions of apical cell surface area and perimeter induced by the pulse, a considerable relaxation event also occurred (Fig. 7C and Fig. S4), which were indeed observed during apical constriction event after single Ca\(^{2+}\) transient in vivo (Fig. 5B). These results suggest that our model reproduced the in vivo situation, in which Ca\(^{2+}\) transients accelerate AC, and hence decreases the tissue size when the stabilization mechanisms is present.

Next, in order to examine the role of Ca\(^{2+}\) transients in decreasing tissue size qualitatively, we gradually changed the pulse number and found that the effect became more pronounced as the total number of pulses was increased independently of the proportion of activated edges per cell (Fig. 7D). In the sparse condition, the relationship between the number of pulses and the constriction rate was a nearly linear dependence (Fig. S6). Next, we concentrated on the spatial and temporal frequencies of the pulse to examine the collectivity effect. In comparing dense versus sparse pulses, we found that dense pulses induced tissue deformation more rapidly within the active period (Fig. 7E,G). However, over the entire course of the simulation, dense pulses were less effective than sparse pulses when the same total number of pulses was used (Fig. 7E,F, Movie 11). The negative effect of collectivity on the decrease in tissue size was attenuated as the proportion of activated edges per cell was decreased (Fig. 7F). However, because almost all of the segments contract in the in vivo situation (Fig. 5A), these data suggest that random Ca\(^{2+}\) fluctuations at the single-cell level
decrease the tissue size more effectively than multicellular, collective Ca\textsuperscript{2+} fluctuations.

In order to examine the robustness of the above results, we analyzed the modified models with varied assumptions (Fig. S5). When the coefficients of elasticity of cell’s apical surface and apical perimeter were assumed to decrease during the pulse, the effectiveness of sparse pulses on decreasing tissue size was observed in the presence of the Acn component (Fig. S5A) similar to the case where the pulse was linked to activation of line tension (Fig. 7E). On the other hand, when the tension fluctuation was induced during the pulse, the decrease in tissue size was not accelerated (Fig. S5B). As another attempt, we analyzed the two modified models in which the natural/preferred area was allowed to increase. The results showed that the effectiveness of sparse pulses on decreasing tissue size was also observed in the presence of the Acn component, although the differences of constriction rate became smaller (Fig. S5C,D). These data suggest that in the conditions that recapitulated the combinational effects \textit{in vivo}, the prediction about the effectiveness of sparse pulses on decreasing tissue size was robust.

In order to validate the prediction from the model simulations \textit{in vivo}, we fitted a linear mixed model with single-cell and multicellular Ca\textsuperscript{2+} transients as explanatory variables and the amount of NTC as a response variable to data of untreated embryos, and obtained estimated contributions of single-cell Ca\textsuperscript{2+} transients and multicellular Ca\textsuperscript{2+} transients to the amount of NTC (Fig. S7 and Supplementary Materials and Methods). As is shown in Table 1, the coefficient of single-cell Ca\textsuperscript{2+} transients (0.072 ± 0.011) was significantly larger than that of multicellular Ca\textsuperscript{2+} transients (0.028 ± 0.011) ($p$-value = 7.231 × 10\textsuperscript{-3}, Student’s $t$-test). These results supported the prediction from the model simulations that the Ca\textsuperscript{2+} fluctuations at the single-cell level more effectively accelerated AC and NTC than did multicellular Ca\textsuperscript{2+} fluctuations \textit{in vivo}. 
DISCUSSION

In this study we show that two types of active Ca\(^{2+}\) signaling patterns modulate apical constriction via cortical F-actin remodeling, and thereby contribute differently to efficient NTC. Our present study and a recent paper (Christodoulou and Skourides, 2015) propose a novel role of active Ca\(^{2+}\) fluctuation in accelerating AC. The trigger for Ca\(^{2+}\) transients, and the mechanism that allow it to propagate through a tissue remain to be investigated. We did not detect any bias in the direction of wave propagation relative to the body axes, whereas the wave propagation in the wound healing response originates from wounded cells (Antunes et al., 2013; Herrgen et al., 2014). Multicellular Ca\(^{2+}\) transients in the NP produced a higher intensity of R-GECO1.0 fluorescence per cell than did single-cell level transients (Fig. 2); therefore, the wave-like propagation of Ca\(^{2+}\) transients at the tissue level might be induced above a particular threshold Ca\(^{2+}\) signal strength. Our study also suggests that eATP regulates both the single-cell and the multicellular Ca\(^{2+}\) transients (Fig. 4). eATP activates downstream signaling in the cell that secreted the ATP (autocrine signaling) and in neighboring cells (paracrine signaling) (Corriden and Insel, 2010; Schwiebert and Zsembery, 2003). Several pathways, including ATP-permeable release channels and ATP-filled vesicles, have been proposed for the secretion of cytosolic ATP, which is triggered by mechanical stimulation or extracellular biochemical cues (Corriden and Insel, 2010; Schwiebert and Zsembery, 2003). Hence, ATP release induced by spontaneous, mechanical stretch or compression might trigger Ca\(^{2+}\) transients and possibly the wave propagation in the developing NP, in which dynamic autonomous and non-autonomous tissue movements take place (Morita et al., 2012; Wallingford and Harland, 2001). In order to dissect more precisely the regulatory mechanisms upstream of Ca\(^{2+}\) transients, functional studies using genome editing, for example, would be useful since pharmacological approaches can be misleading due to off-target effects (Bootman et al., 2002; Xu et al., 2005).

Although multicellular Ca\(^{2+}\) transients have been shown to accelerate closure process during wound healing (Antunes et al., 2013; Herrgen et al., 2014), the contribution of random single-cell Ca\(^{2+}\) fluctuations to epithelial remodeling has been elusive, probably because the effect of these transients is too small at the tissue level to be examined experimentally. Moreover, since the temporal patterns of single-cell Ca\(^{2+}\) fluctuations varied among embryos (Fig. 3B-E), it might be regulated by mechanisms that are inherently noisy or heterogenous, further complicating efforts to draw general conclusions about its functional significance. In this study, we used a cell-vertex mathematical model in surface view to investigate how distinct Ca\(^{2+}\) fluctuation patterns affect AC and persistent epithelial remodeling (Figs 6,7).
Computational simulations using this model showed that pulsed contractions accelerate the decrease in tissue size even in the sparse condition, suggesting that Ca\(^{2+}\)-induced AC always contributes positively to NTC. Our mathematical and statistical analyses also suggest that spatially and temporally random Ca\(^{2+}\) transients at the single-cell level function to reduce the overall tissue size more effectively than multicellular, collective Ca\(^{2+}\) fluctuations, making them cost-effective for normal NTC. On the other hand, the multicellular, wave-propagated Ca\(^{2+}\) transients might be useful when tissue must be closed quickly, as in wound healing. Since the number of single-cell Ca\(^{2+}\) transients increases in the late phase of NTC, a genetic program that represses collectivity and promotes the randomization of Ca\(^{2+}\) fluctuations may exist to ensure that embryos are able to undertake their primitive CNS formation under physiological conditions. In summary, the Ca\(^{2+}\)-dependent mechanisms highlighted in this study might be acting, in parallel with known pathways controlling AC, such as the Shroom3 or Wnt/PCP pathway, as a compensatory system to avoid incomplete NTC, which is the second most frequent congenital malformation in humans (Copp et al., 2003).
MATERIALS AND METHODS

Ethics statement
All protocols for animal care and experiments were approved by the Institutional Animal Care and Use Committee of the National Institutes of Natural Sciences, Japan, and were performed in accordance with institutional guidelines for the care and use of laboratory animals.

Injections, morpholinos, and RNA expression constructs
Experiments with *Xenopus laevis* embryos were performed as previously described (Suzuki et al., 2010). After injection, the embryos were cultured in 3% Ficoll/0.1× Steinberg’s solution until stage 9, then washed and cultured in 0.3× Marc’s Modified Ringer’s (MMR) until the appropriate stage for analysis (Nieuwkoop and Faber, 1967).

Antisense Mo (Gene Tools) was injected into embryos at the four-cell stage (17 ng per embryo). The Mo sequences were as follows: N-cadherin Mo

5’-GAAGGGCTCTTTCCGGCACA TGGTG-3’ (Nandadasa et al., 2009); 5mis-N-cadherin Mo, 5’-GAAcGGgTCTTTgCGcCACA TcGTG-3’.

Capped sense RNAs were synthesized with the mMESSAGE mMACHINE kit (Ambion), purified on a NICK column (GE Healthcare), and injected into embryos at the four-cell stage. All ORFs were cloned into the pCS2p+ vector. Embryos received injections of RNA constructs in the following amounts: R-GECO1.0 (Zhao et al., 2011) and G-GECO1.2 (Zhao et al., 2011), 1 ng per embryo; YC-Nano50 (Horikawa et al., 2010), YC-Nano30 (Horikawa et al., 2010), and YC-Nano15 (Horikawa et al., 2010), 500 pg per embryo. Cell surface–targeted ATeam3.10 (AT3.10-GPI) and its RK mutant were generated by fusing ATeam3.10 (Imamura et al., 2009) or its RK mutant (Imamura et al., 2009) with the signal peptide sequence and the GPI-anchor domain of *Xenopus* glypican4 (Ohkawara et al., 2003), and 1 ng was injected per embryo. EGFP was injected at 100 pg per embryo.

Membrane-targeted EGFP and mRFP were generated by fusing the farnesylation signal of c-Ha-Ras to the C terminus of EGFP and mRFP, respectively, and 100–200 pg was injected per embryo. Lifeact-EGFP (Riedl et al., 2008) was injected at 180 pg per embryo. *Xenopus* E-NTPDase1 and its mutant version in which the enzymatic active site was deleted (ΔACR) were injected at 100–200 pg per embryo.
**Chemical treatments**

For inhibitor treatments, 100× stocks of 2APB (D9754; Sigma) and nifedipine (145-05781; Wako) in DMSO were added to the medium at stage 13, to concentrations of 25 µM and 200 µM, respectively. For uncaging experiments, NPE-caged IP$_3$ (I23580; Molecular Probes) was injected into embryos at the four-cell stage (5 pmol per embryo). DMNPE-caged ATP (A1049; Molecular Probes) was added to the medium to a concentration of 100 µM.

**In situ hybridization and F-actin staining**

In situ hybridization was performed as previously described (Suzuki et al., 2010). The following plasmids were used for probe synthesis: Sox2 (XL039o24; XDB3); N-cadherin (XL289n05ex; XDB3); and Epidermal keratin (XL056e18; XDB3). For F-actin visualization, embryos were fixed in MEMFA and stained with Alexa 546-phalloidin (A22283; Molecular Probes).

**Confocal imaging**

Devitellinized embryos were mounted on an agarose-coated glass-base dish (3910-035; AGC, Japan) filled with 0.3× MMR. Confocal fluorescence images were acquired as a z-series of 512 × 512 pixels using a spinning-disc confocal unit (CSU-X1; Yokogawa, Japan) with an EMCCD camera (iXon3; Andor) and 455-, 488-, and 561-nm lasers (Andor) on an inverted microscope (IX81; Olympus) with a 10× (UPlanSAPO 10×/0.4; Olympus) or 20× (UPlanAPO 20×/0.7; Olympus) objective lens at a room temperature adjusted to 18–20 °C. Unless otherwise noted, we observed the R-GECO1.0 fluorescence at 20 or 40-second intervals for up to 6 hours.

For UV illumination in uncaging experiments, mercury lamp–based epifluorescent optics with a band-pass filter (AT350/50x; Chroma) were inserted into the path of the excitation light, and the duration of illumination was controlled by iQ2 software (Andor). For the photolysis of NPE-caged IP$_3$, the samples were illuminated for 3 seconds by a UV light reduced with a 6% neutral-density filter (32-ND6; Olympus). For the photolysis of DMNPE-caged ATP, the samples were illuminated for 20 seconds by unreduced UV light.

Image processing and analyses were done with the ImageJ (NIH) and R (www.r-project.org). All quantifications used the maximum intensity projection of the z-series. Details are provided in Supplementary Materials and Methods.
**Mathematical model**

The mathematical model constructed in this study is based on the vertex model (Farhadifar et al., 2007; Nagai and Honda, 2001; Okuda et al., 2013; Rauzi et al., 2008). The simulations were programmed in C. Details are provided in Supplementary Materials and Methods.

**Illustrations and statistical analyses**

Figures were assembled with Photoshop (Adobe), Illustrator (Adobe), and PowerPoint (Microsoft). Data plots and statistical analyses were performed in Excel (Microsoft) and R. Data sets were subjected to Shapiro-Wilk test to determine distributions. No statistical method was used to predetermine sample size. The experiments were not randomized. The investigators were not blinded to allocation during experiments and outcome assessment.
Acknowledgements
We thank the Data Integration and Analysis Facility, and the Spectrography and Bioimaging Facility in NIBB Core Research Facilities for technical support; members of the N.U. laboratory, S. Nonaka laboratory, and N. Shiina laboratory for valuable discussions and comments.

Competing interests
The authors declare no competing or financial interests.

Author Contributions
M.S., M.S., H.K., Y.H., T.F., and N.U. designed research; M.S., H.K., Y.H., and N.Y. performed research; M.S., M.S., H.K., K.H., H.I., T.N., and R.E.C. contributed new reagents/analytic tools; M.S., M.S., H.K., Y.H., and N.Y. analyzed the data; and M.S., M.S., H.K., R.E.C., and N.U. wrote the paper.

Funding
This work was supported by KAKENHI [10533193 and 15KT0154 to M.S., 22127007 and 15H05865 to N.U.] from the Japan Society for the Promotion of Science (JSPS).
References


**Figure 1. Intracellular Ca\(^{2+}\) is required for Xenopus neural tube closure.**

(A) Dorsal views of embryos at stage 16 treated with DMSO, 25 µM 2APB, and 200 µM nifedipine. Dashed lines indicate the outlines of the NP. (B) The mean width of the NP in embryos visualized by the expression of the pan-neural marker gene Sox2. Error bars depict s.e.m. The number of embryos examined is shown on each bar. **P<0.01 and ***P<0.001 compared with the DMSO-treated control; two-sided Welch’s t-test. (C) Transverse sections of stage 16 embryos stained with Phalloidin (Top) and outlines of neural tissues and cells (Bottom). Scale bars, 100 µm. (D) Apical width of stage 16 embryos. Black line indicates the median value. **P<0.01 and ***P<0.001, two-sided Mann-Whitney U test; n = 54 cells.
embryos (DMSO); 97 cells, 12 embryos (2APB); 88 cells, 12 embryos (nifedipine). (E) In situ hybridization analysis of inhibitor-treated embryos. Dorsal views showing the expression of Sox2, a pan-neural marker (top), N-tubulin, which marks differentiated neurons (middle), and Epidermal keratin, an epidermal marker (bottom). Anterior is to the top. The expression patterns were similar in inhibitor-treated embryos and DMSO-treated controls, but the expression domains were wider in the inhibitor-treated embryos because of delayed NTC.
Figure 2. Live-imaging analyses of intracellular calcium ions in the neural plate.

(A) A Ca$^{2+}$ transient at the single-cell level, visualized with R-GECO1.0 (gray), in a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. R-GECO1.0 was introduced on the left side of the embryo. The midline is indicated by a dotted line. Time course of four sample cells is shown in the right panels. Scale bar, 100 µm. (B) Time-lapse imaging data of a multicellular, wave-like Ca$^{2+}$ transient in the embryo shown in (A). (C) Fluorescence intensities of cytoplasmic R-GECO1.0 over time; the light color indicates the s.d. In multicellular Ca$^{2+}$ transients (red), cells adjacent to the cell that was initially activated were measured (n = 6 cells). (D) The radius and velocity of wave propagations in multicellular Ca$^{2+}$ transients. The red line represents the relationship between the two data sets, calculated using the least-squares method of linear regression (n = 21 cells, 5 embryos).
Figure 3. Quantitative analyses of intracellular Ca\(^{2+}\) activities in the neural plate.

(A) Representative results of quantitative analyses of a Ca\(^{2+}\) fluctuation in an untreated (left), 2APB-treated (middle), and nifedipine-treated (right) embryo. R-GECO1.0 and EGFP were introduced to the left side of the NPs. (Top) EGFP fluorescence images at the start of time-lapse...
recording; (middle) time projections of Ca\(^{2+}\) activity (R-GECO1.0/EGFP); and (bottom) time projections of reconstructed circles corresponding to the area of the Ca\(^{2+}\) transient, extracted by image processing. Solid yellow lines indicate the midline; dotted lines indicate the border between neural and non-neural tissues. The reconstructed circles were color-coded based on the quartiles of the area distributions in an untreated embryo. (B) The mean number of Ca\(^{2+}\) transients during NTC. Time interval of observations is 20 seconds. The data are shown as smoothed curves, obtained by averaging the originally counted numbers at a given time point with those of neighboring time points (50 time points total). The light color indicates the s.d. (C) The number of single-cell Ca\(^{2+}\) transients in the early and late phases of NTC. **P<0.01 and ***P<0.001, two-sided Mann-Whitney U test. (D) Number of multicellular Ca\(^{2+}\) transients in the early and late phases of NTC. **P<0.01, two-sided Mann-Whitney U test. (E) Ratio of the total area of the multicellular/single-cell Ca\(^{2+}\) transients in the early and late phases of NTC in untreated embryos. ***P<0.001, two-sided Wilcoxon signed rank test. (F) Representative data for the closing speed (black) and the total R-GECO1.0 intensity values at the tissue level (red) during NTC. The closing speed is shown as a smoothed curve, obtained by averaging the rate determined from image analyses (gray) at a given time point with those of neighboring time points (10 time points total). Overlaps between temporary increases in closing speed and intense Ca\(^{2+}\) transients are highlighted (yellow). (G) Mean cross-correlation coefficients between the closing speed and the total R-GECO1.0 value. The light color indicates s.d. n = 19 (untreated), 5 (2APB-treated), and 6 (nifedipine-treated) embryos. Results in (B)-(E), and (G) are for the same data set.
Figure 4. Extracellular ATP in Ca\(^{2+}\) fluctuation and neural tube closure.

(A) Mean number of Ca\(^{2+}\) transients in embryos expressing an E-NTPDase1 mutant (ΔACR; red) or E-NTPDase1 (NTPDase1; green), shown as smoothed curves obtained by averaging the originally counted values at a given time point with those of neighboring time points (25 time points total). Time interval of observations is 40 seconds. Light color indicates the s.d. 

(B) Number of single-cell Ca\(^{2+}\) transients in the early and late phases of NTC. *P<0.05, two-sided Mann-Whitney U test. 

(C) Number of multicellular Ca\(^{2+}\) transients in the early and late phases of NTC. *P<0.05, two-sided Mann-Whitney U test. 

(D) The mean cross-correlation between the closing speed and the total R-GECO1.0 value in embryos expressing a mutant E-NTPDase1 (ΔACR; red) or E-NTPDase1 (NTPDase1; green). The light color indicates s.d. 

n = 3 (ΔACR), 5 (NTPDase1) embryos. Results in (A)-(D) are for the same data set. 

(E) Images showing the yellow/cyan fluorescence ratio of AT3.10-GPI on the surface of NP cells, by FRET analysis. The mean ratio was measured from the masked region generated by membrane-targeted mRFP (right). Scale bar, 30 µm. 

(F) The mean yellow/cyan fluorescence ratio of AT3.10-GPI on cell surfaces in the NP by FRET analysis. The number of embryos examined is indicated in each bar. **P<0.01 and ***P<0.001, two-sided Welch’s t-test.
Figure 5. Relationship between Ca^{2+} fluctuation and apical constriction.

(A) Dynamics of intracellular Ca^{2+} and F-actin at the single-cell level. An embryo expressing R-GECO1.0 (top) and Lifeact-EGFP (middle) was imaged during neural tube closure. The numbers in the top panels (+0-160) indicate time (seconds) corresponding to the 340–500 second range in (B). Numbers shown in the cell outlines (bottom) indicate the apical cell area (%) relative to that at time 0 in (B). (B) Temporal profiles of the mean fluorescent intensities of R-GECO1.0 (red) and medial Lifeact-EGFP (green), and the relative apical cell area (blue) in a single cell. The light color indicates the s.d. Period shown in (A) is highlighted in yellow. (C) Mean cross-correlation coefficients between the temporal dynamics of the apical cell area (blue), medial Lifeact-EGFP (green), and R-GECO1.0 (n = 8 transients, 4 cells, 1 embryo). The light color indicates s.d. (D) Relative apical cell area 50 seconds after photolysis of NPE-caged IP_{3} in the NP. Red line indicates the median value. *P<0.05, two-sided
Mann-Whitney U test; n = 26 cells, 2 embryos (-UV); 29 cells, 2 embryos (+UV). (E) Relative apical cell area 50 seconds after photolysis of DMNPE-caged ATP in the NP. Red line indicates the median value. **P<0.01 and ***P<0.001, two-sided Mann-Whitney U test; n = 42 cells, 4 embryos (-DMNPE-caged ATP); 44 cells, 4 embryos (+DMNPE-caged ATP); 39 cells, 4 embryos (5mis-N-cadherin Mo; +DMNPE-caged ATP); 40 cells, 4 embryos (N-cadherin Mo; +DMNPE-caged ATP).
Figure 6. Schematic representation of the vertex model.

(A) The mechanical potentials are shown with five cells. (B) Effect of the Ca$^{2+}$ transient is described. The Ca$^{2+}$ transients at the single-cell (i) and multicellular (ii) levels are shown. Cells marked by blue stars are activated. Activated cellular edges in an activated cell are marked by arrows (iii). (C,D) The constrictive nature of apical cell surface with a ratchet-like stabilization is modeled by two differential equations. The regulations of the natural cell area and of the natural cell perimeter are described in (C) and (D), respectively. The bright orange regions in (C) are the actual cell surface area, and the dark orange regions correspond to the natural cell surface area. The bright orange lines in (D) are the actual cell perimeter and the dark orange broken lines correspond to the natural perimeter. See main text and Supplementary Materials and Methods for the detail.
Figure 7. Mathematical analysis of pulsed apical constriction.

(A) Mean tissue sizes of the modeled epithelial sheets during the time course of the simulations, and representative images at the end of each simulation. (B) Mean apical constriction at the end of the simulations. In (A) and (B), the pulsed contractions were introduced at a frequency of 0.025 simulation time$^{-1}$ edge$^{-1}$, and all of the cell edges in the activated cells were contracted. ***P<0.001, two-sided Student’s t-test. (C) Mean line tension, potential energy from the elasticity of apical surface area, area, and natural area of single cell (#58) during the time course of the simulations with the pulse and Acn components. Period with pulse is highlighted in yellow. See Supplementary Materials and Methods for definition. (D) Relationship between the pulse frequency and mean constriction at the end of the simulations. The proportion of cell edges undergoing contraction per cell was set to a probability ($p_e$) 1, 0.5, or 0.25. (E) Mean tissue sizes during the time course of the simulations, when the active period in which the pulses were introduced was set from 200 to 2000 simulation times. (F,G) The mean constriction at the end of the simulations and the constriction rate during the active period,
when the length of the active period and the proportion of the cell edges undergoing contraction per cell were changed. All error bars depict s.d; n = 5 different initial conditions. Details of the models and the simulation processes are described in Supplementary Materials and Methods.
Table 1. Statistics for fixed effects of the mixed linear model.

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*Zero values were excluded for calculation.
Supporting Information

Supplementary Materials and Methods

Image processing and analyses
Quantitative analyses of the cellular morphology were performed as previously described (Suzuki et al., 2010). To determine the radius and velocity of multicellular Ca\(^{2+}\) transients, the edges of the wave propagation were manually determined at each time point. The radius was calculated as the maximum distance between the edges and the initially activating cells, and 2–6 values for velocity in a single propagation were averaged.

To obtain signal intensities and the size (area) of Ca\(^{2+}\) fluctuations, R-GECO1.0 and EGFP images were subjected to the normalization of R-GECO1.0 fluorescence. The signal intensity of R-GECO1.0 is affected by the amount of transfected R-GECO1.0 mRNA. The homogeneous transfection of mRNA throughout a Xenopus embryo presents a technical challenge. To overcome this problem, we co-injected mRNA encoding EGFP as a loading control to estimate the transfection efficiency of the R-GECO1.0 mRNA. The R-GECO1.0 and EGFP signal intensities in raw images were correlated spatially and quantitatively. Using this relationship between the reporter signal intensities, transfection biases on the R-GECO1.0 signal intensity could be estimated from the EGFP signal intensity. We performed linear regression using the R-GECO1.0 and EGFP signal intensities at each pixel as observatory and explanatory variables, respectively, and used the residual values for downstream data preprocessing as the normalized R-GECO1.0 signal intensities. This method using the intense fluorescence intensity of the GECO proteins minimizes false positive signals due to its heterogeneous expression level, and allows for increased imaging speed. The data preprocessing was implemented with Perl (www.perl.org), R, and ImageJ (the custom scripts are available here: https://github.com/masanaolab/calcium). The normalized R-GECO images were blurred using the smooth filter in ImageJ for noise reduction. Then particle analyses were performed with a masked region generated by auto-thresholded (Huang’s method implemented in ImageJ) EGFP images with the smooth filter applied. The threshold values for the R-GECO ratio and particle size were
set to 1.25 and 50 pixels (1 pixel = 1.33 µm), respectively. Particles larger than 500 pixels were defined as multicellular Ca\(^{2+}\) transients. Additional inspection removed false-positive particles in the automated preprocessing. Time-series were trimmed to match the timing of NTC completion before further analyses.

Cross-correlation analyses of R-GECO values with apical cell-area dynamics, medial F-actin dynamics, and the closing movement of NTC were done to obtain the Spearman's rank correlation coefficient and time delay. The speed of NTC was determined by measuring the mean width of the EGFP-expressing area from auto-thresholded EGFP images with a smooth filter applied. We performed a linear fit of the closing speed of the NTC and used the residuals for the analyses in order to remove long time scale trends. The total R-GECO1.0 intensity values at the tissue level were determined from the total fold changes of normalized R-GECO ratio in extracted particles. For cellular analyses, apical cell morphologies were determined manually. The medial F-actin and R-GECO values were measured from a defined circular region of interest that excluded cell boundaries.

To measure FRET in the neural plate, two emission images for donor and acceptor emission were acquired upon donor excitation with a 455-nm laser, using embryos at stage 14–15. To measure the intracellular Ca\(^{2+}\) concentration, the yellow Cameleon-Nano (YC-Nano) (Horikawa et al., 2010) ultrasensitive Ca\(^{2+}\) indicators, which have a \(K_d\) of 50, 30, or 15 nM, were expressed with membrane-targeted mRFP. The raw images were blurred with the smooth filter. The yellow/cyan fluorescence ratio was measured from the masked region generated by an auto-thresholded image of the membrane-targeted mRFP that included both cell membranes and cytoplasmic domains. To measure the extracellular ATP concentrations, cell-surface-targeted ATeam3.10 (AT3.10-GPI) and its RK mutant were expressed with membrane-targeted mRFP in the neural plate. The raw images were blurred with the smooth filter, followed by background subtraction with a rolling-ball algorithm implemented in ImageJ. The yellow/cyan fluorescence ratio was measured from the masked region generated by a manually thresholded image of the membrane-targeted mRFP to exclude the cytoplasmic domain.
Construction of a mathematical model

Overview of the vertex model

As the aim of this mathematical analysis was to address the general effect of Ca\textsuperscript{2+} fluctuations on a tissue’s apical constriction, we considered a simplified situation using a two-dimensional cell sheet consisting of 256 cells with no defined tissue polarities (although NTC involves three-dimensional morphological changes in tissue and cells that have planar anterior-posterior and dorso-ventral cell polarities). Our analyses evaluated the overall shrinkage in the apical surface area, but not the directional or polarized shrinkage of the tissue.

In our vertex model, we considered the following mechanical components: the line tension generated on each edge of the cell, the elasticity of the cell’s apical perimeter, and the elasticity of the cell’s apical surface area (Fig. 6A), all of which are often adopted in vertex models (Farhadifar et al., 2007; Nagai and Honda, 2001; Okuda et al., 2013; Rauzi et al., 2008). The mechanical potential energies derived from these three components were defined as described (see Definition of the mechanical potential energy).

Ca\textsuperscript{2+} transient occurs in each cell and changes the localization of cytoskeletal proteins in the cell (Fig. 5). Thus, a Ca\textsuperscript{2+} transient would temporally regulate certain mechanical parameter(s) in the cell. We assumed that Ca\textsuperscript{2+} transient modifies the line tension of the cellular edges (see Definition of the activation of line tension.)

A temporary increase in line tension would decrease the apical surface area of the tissue and of the individual cells. However, after the line tension returns to baseline, the apical surface areas of the tissues and cells recover (see Fig. 7A,B, +Pulse -Acn.). On the other hand, in neural tube closure in vivo, the apical surface area of the tissue gradually decreases and is not recovered. Thus, the apical cell surface has a constrictive nature without accompanying the restoration of the surface area. A possible mechanism for maintaining the decrease in the apical surface area without the restoration is a ratchet-like mechanism that stabilizes the apical cell membrane that had been recently reported (Martin and Goldstein, 2014; Mason et al., 2013), such that once the cell’s apical surface shrinks, the surface area does not recover. In other words, the apical surface of a cell has the potential to decrease in surface area, but not to increase. We introduced a constrictive nature of apical cell surface with a ratchet-like stabilization.
(see Definition of a constrictive nature of apical cell surface with a ratchet-like stabilization). We did not consider cell proliferation or cell death, but did consider a cell-cell junctional rearrangement called the T1 process (Farhadifar et al., 2007; Nagai and Honda, 2001).

**Definition of the mechanical potential energy**

We defined the potential energies derived from three mechanical components. The total potential energy $U$ is shown as follows:

$$U = U_A + U_P + U_L \quad \text{eq. 1},$$

where $U_A$, $U_P$, and $U_L$ are the potentials derived from the elasticity of a cell’s apical surface area, the elasticity of the cell’s apical perimeter, and the line tension generated on each edge of the cell, respectively (Fig. 6A). $U_A$ is defined as follows:

$$U_A = \sum_{n}^{\text{cell}} \frac{K^A_n}{2} \left( \frac{A_n}{A^0_n} - 1 \right)^2 A^0_n \quad \text{eq. 2},$$

where $A_n$ and $A^0_n$ are the cell’s apical surface area and its natural/preferred apical surface area, respectively, and $K^A_n$ is the coefficient of elasticity. $U_P$ is defined as follows:

$$U_P = \sum_{n}^{\text{cell}} \frac{K^P_n}{2} \left( \frac{P_n}{P^0_n} - 1 \right)^2 P^0_n \quad \text{eq. 3},$$

where $P_n$ and $P^0_n$ are the cell’s apical perimeter and its natural/preferred apical perimeter, respectively, and $K^P_n$ is the coefficient of the elasticity. In eq.2 and 3, the potentials are described by using the strains of the cell area and the perimeter (ratios of $A_n$ to $A^0_n$ and of $P_n$ to $P^0_n$, respectively) as previously reported (Okuda et al., 2013), but not by using the amounts of the deformations of the cell area and the perimeter (subtraction of $A^0_n$ from $A_n$ and of $P^0_n$ from $P_n$). These definitions enabled us to simulate cell behaviors even when the natural cell area and/or the natural perimeter are largely changed. $U_L$ is defined as follows:

$$U_L = \sum_{n}^{\text{cell edge}} \sum_{<ij>} T_n^{<ij>} L_n^{<ij>} \quad \text{eq. 4},$$

where $T_n^{<ij>}$ and $L_n^{<ij>}$ are the line tension and the length of each cellular edge connecting the $i$th and $j$th vertices, respectively. A cell-cell junction is formed by the
adhesion of two cells, and is thus composed of two cellular edges derived from the two associating cells. Therefore, the line tension on a cell-cell junction is determined by the sum of the two line tensions derived from the two cellular edges.

We assumed that the inertial effect was negligible, and thus, the force exerted on the \(i\)th vertex \(F_i\) was calculated as follows:

\[
F_i = \mu \frac{dr_i}{dt} = -\frac{\partial U}{\partial r_i}
\]
eq 5,

where \(r_i\) is the positional vector of the \(i\)th vertex, \(\mu\) is the viscosity coefficient of the tissue, and \(t\) is time.

**Definition of the activation of line tension**

The \(\text{Ca}^{2+}\) transient-induced activation of line tension is modeled as follows. Cells are selected as activated according to a predefined parameter \(p_c\), where \(p_c\) is the frequency of cell activation per unit of time (Fig. 6B-i,ii). Then, each cellular edge in the activated cells is activated by a predefined probability \(p_e\) (Fig. 6B-iii). Finally, the line tension on the activated cellular edge is modified. For each simulation, we set the period during which cell activation can be induced; thus, in some simulation conditions, cells are activated for part but not all of the simulation period (Fig. 7E-G; active period).

We modeled the activation induced by two distinct types of \(\text{Ca}^{2+}\) transients by setting the \(p_c\) value: setting a low \(p_c\) produced a sparse population of activated cells, corresponding to \(\text{Ca}^{2+}\) transients in single cells, and setting a high \(p_c\) produced a dense population of activated cells, mimicking multicellular \(\text{Ca}^{2+}\) transients (Fig. 6B-i,ii). Here, we called the former case “random” and the latter case “collective” (Fig. 6B). In both cases, the activation (here called a “pulse”) is induced at the single-cell level, but the density of activated cells differs between the two cases. When \(p_c\) is set to 0.2, a cell is activated 0.2 times per time unit. Thus, if the simulation time period \(t\) is 100, a cell is activated 20 \((p_c \times t)\) times on average.

In an activated cell, some cellular edges are activated, which modulates the line tensions. Which cellular edges will be activated is regulated by \(p_e\) \((1 \geq p_e \geq 0)\). When \(p_e\) is set to 1.0, all cellular edges in the activated cell will be activated (Fig. 6B-iii). If \(p_e\) is set to 0.17 or 0.5, for example, a cell with six edges will have one or three activated edges on average (Fig. 6B-iii).
The line tension on the activated cellular edge is given by

\[ T_n^{<ij>} + \xi \]

\text{eq. 6,}

Where \( \xi \) is a uniform random number from \( \sigma_1 \) to \( \sigma_2 \). Once an edge is activated and \( \xi \) is initially set to a certain value, \( \xi \) is constant until the end of the activation. The results of simulations in which \( \sigma_1 \) and \( \sigma_2 \) were set to the same value are shown in this study since different \( \sigma \) values did not affect the relationship between \( p_c \) and constriction rate of tissues qualitatively (Data not shown). After the activation terminates, the line tension returns to \( T_n^{<ij>} \). The duration time of a single activation is \( \tau \), which is predefined for each simulation.

During simulations, it can happen that a new pulse (activation of a cell) is induced at a cell that is already in an activated state from a previous pulse. In such a case, the effect of the new pulse is essentially added to that of the old pulse. If a cellular edge that was not activated by the old pulse is selected by the new pulse, the line tension will be modified according to eq. 6 with the duration time \( \tau \). If a cellular edge that is activated from a previous pulse is selected again by the new pulse, the duration time is prolonged by adding \( \tau \).

Definition of a constrictive nature of apical cell surface with a ratchet-like stabilization

To model a ratchet-like stabilization mechanism, we focused on both the cell’s natural surface area \( A_0^n \) and the cell’s natural perimeter \( P_0^n \). We assumed that \( A_0^n \) could be decreased but not increased. In other words, once \( A_0^n \) decreases, it will never recover to the original area. The decrease in \( A_0^n \) was assumed to be determined relative to the cell surface area \( A_n \); when \( A_0^n \) is sufficiently large in comparison with \( A_n \), \( A_0^n \) tends to decrease (Fig. 6C). We modeled these properties by defining a differential equation of \( A_0^n \) as follows:

\[ \frac{dA_0^n}{dt} = \kappa_A (A_n - \omega_A A_0^n) \]

\[ = 0 \]

\text{if} \ (A_n - \omega_A A_0^n) < 0 \]

\text{if} \ (A_n - \omega_A A_0^n) \geq 0 \]

\text{eq. 7,}

where \( \kappa_A \) is the rate constant, and \( \omega_A \) is a parameter to define a threshold that determines whether \( A_0^n \) should be decreased or not. To prevent \( A_0^n \) from increasing, we defined the equation so that the value of \( dA_0^n/dt \) should be \( \leq 0 \). In normal simulation conditions, \( A_0^n \)
is larger than \( A_n \). Thus, when \( \omega_A \) is 1.0, \( A^0_n \) will always decrease. In general, \( A^0_n \) will tend to decrease in the case where \( \omega_A \) is high, but will not in the case where \( \omega_A \) is low.

We adopted a similar assumption for \( P^0_n \), as follows:

\[
\frac{dP^0_n}{dt} = \kappa_P (P_n - \omega_P P^0_n) \quad \text{if} \quad (P_n - \omega_P P^0_n) < 0
\]
\[
= 0 \quad \text{if} \quad (P_n - \omega_P P^0_n) \geq 0 \quad \text{eq. 8},
\]

where \( \kappa_P \) is the rate constant, and \( \omega_P \) is a parameter to define a threshold that determines whether \( P^0_n \) should decrease or not (Fig. 6D). To prevent the cell surface area \( A_n \) from becoming less than 0, minimum values of \( A^0_n \) and \( P^0_n \) are limited to 0.3 and 2.0, respectively.

In summary, our model is composed of the combination of the mechanical potential defined in eq.1 and the differential equations defined in eq.7 and 8. If neither eq. 7 nor 8 is introduced, the apical surface area of the tissue will recover after the activation of line tensions ends (Fig. 7A,B).

**Simulation processes and conditions**

**Initial cell configurations**

Initial cell configurations were generated using Voronoi diagrams and subsequent simulations of our model without the constrictive nature of apical cell surface. In our initial conditions, cells were positioned in an almost circular region. We independently generated five initial conditions, and used these in our analyses.

**Simulation**

Simulations were performed according to eq. 5 using the Euler method. Eq. 7 and 8 were also numerically solved by the Euler method. Parameter values are shown in Tables S1 and S2. The simulations were programmed in C.

**Statistical validation of prediction from simulation**

Temporal profiles of closing movement, the total area of single-cell \( \text{Ca}^{2+} \) transients, and multicellular \( \text{Ca}^{2+} \) transients from each untreated embryo during last 200 minutes before the completion of NTC (Fig. S7A) were divided into twenty time windows (10 minutes each) (Fig. S7B). The amount of NTC was calculated as the difference of
EGFP-expressing area between start and end points of time windows. Then by using all of the observed data (n= 19 embryos, 380 time windows), a mixed linear model was fitted to the data:

\[ C_{smne} = S_{ne} + M_{ne} + N_{e} + (1|E_{e}) + \epsilon_{smne}, \]

where \( C, S, M, N, E, \) and \( \epsilon \) are amount of NTC, total area of single-cell Ca\(^{2+}\) transients, total area of multicellular Ca\(^{2+}\) transients, time window number, embryo, and residual, respectively. \( S, M, \) and \( N \) are fixed effects, and \( E \) and \( \epsilon \) are random effects (Fig. S7C). In order to examine whether single-cell Ca\(^{2+}\) transients and multicellular Ca\(^{2+}\) transients differentially contributed to the amount of NTC, the difference between estimated coefficients of them was analyzed by the Student’s \( t \)-test. The standard error appropriate for the difference of coefficients was calculated using the standard errors of coefficients obtained from the model fitting.
Table S1. Fixed parameter values in the simulations.

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Supplementary Figures

Figure S1. Neural tube closure in *Xenopus laevis*.

(A) Time-lapse imaging data of the neural tube closure of a *Xenopus laevis* embryo, dorsal views. The elapsed time (minutes) is shown at the bottom right of each panel. (B) A transverse section through the neural plate of a stage-16 embryo, stained with phalloidin. Right: illustration of NP cells in the surface layer undergoing apical constriction.
Figure S2. Method of the live-imaging analyses of neural tube closure.

(A) Schematic of *Xenopus* embryo microinjection and confocal experiments. GECO RNAs were injected into the presumptive neural region in embryos at the four-cell stage. The embryos were then cultured to the appropriate developmental stage, after which the vitelline membranes were removed. The embryos were mounted in a hand-made agarose gel chamber on a glass-base dish filled with 0.3x MMR, and were observed by an inverted microscope equipped with a spinning-disk confocal unit and an EM-CCD camera. (B) Workflow for the quantitative imaging analyses of Ca²⁺ dynamics in the neural plate (see Materials and Methods for the detail.)
Figure S3. Supplementary profiles of Ca\textsuperscript{2+} fluctuation.

(A) The number of Ca\textsuperscript{2+} transients occurring during NTC in the individual embryo shown in Fig. 3. Plots are shown as smoothed curves of the original counts by averaging values at a given time point with neighboring time points (50 time points total). (B) The mean yellow/cyan fluorescence ratio of the FRET-based Ca\textsuperscript{2+} indicators YC-Nano50, YC-Nano30, and YC-Nano15 in the neural plate in embryos treated with calcium-channel inhibitors. Error bars depict s.d. The number of embryos examined is shown on each bar. Statistical significances were assessed by two-sided Student’s \textit{t} test. (C) The number of Ca\textsuperscript{2+} transients during NTC in the embryo shown in Fig. 4. The plot is shown as smoothed curves obtained by averaging the originally counted numbers at a given time point with those of neighboring time points (25 time points total).
Figure S4. Temporal changes in parameters of single cell in modeled epithelial sheet.

Mean line tension, potential energy from line tension, potential energy from the elasticity of apical surface area, potential energy from the elasticity of apical perimeter, apical surface area, apical perimeter, natural area, and natural perimeter of single cell (#58) during the time course of the simulations with the combination of pulse and Acn components. Arrows indicate periods with pulses.
Figure S5. Mathematical analysis of pulsed apical constriction with varied assumptions.

Mean tissue sizes of the modeled epithelial sheets during the time course of the simulations with the Acn component alone (black), and with the Acn components and the pulse whose active period was set from 200 to 2000 simulation times (colors). Basis of parameter values in the simulations is the same with Figure 7A (#2,4 in Table S2) and 7D (#43-46 in Table S2). (A) During the pulse, the coefficient of elasticity of cell’s apical surface area and perimeter are changed instead of the line tension; $K_{an}^l = 0.2$; $K_{an}^p = 0.15$. (B) $\sigma_1 = -0.1$; $\sigma_2 = 0.1$. (C) The cells’ natural surface area and the cells’ natural perimeter are permitted to increase: eq.7 and 8 were simplified to become $\frac{dA_n}{dt} = \kappa_A(A_n - \omega_AA_0)$ and $\frac{dP_n}{dt} = \kappa_p(P_n - \omega_PP_0)$; $\omega_A = 0.7$; $\omega_P = 0.8$. (D) The cells’ natural surface area and the cells’ natural perimeter are permitted to increase as shown in (C); $\omega_A = 0.8$; $\omega_P = 0.7$. 
Figure S6. Relationship between pulse number and constriction rate in sparse condition.

A magnified plot of mean constriction at the end of the simulations in Fig. 7D. The proportion of cell edges undergoing contraction per cell was set at probability ($p_e$) 1 (black), 0.5 (cyan), and 0.25 (red). Condition without pulse is also shown (blue). Error bars depict s.d; $n = 5$ different initial conditions. Details of the models and the simulation processes are described in Supplementary Materials and Methods.
Figure S7. Schematic workflow for statistical validation of prediction from simulation using observations in vivo.

(A) Temporal profiles of closing movement, the total area of single-cell Ca$^{2+}$ transients, and multicellular Ca$^{2+}$ transients during last 200 minutes before the completion of NTC.

(B) Generation of data set for statistical analysis by dividing temporal profiles into twenty time windows. (C) Fitting mixed linear model to the data set to estimate contributions. See Supplementary Materials and Methods for the detail.
Movie 1. Intracellular Ca\textsuperscript{2+} dynamics in the neural plate.

An embryo expressing R-GECO1.0 was imaged during the closure of the neural tube. Imaging shows a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (minutes: seconds) is shown at the top left. Frames were captured every 20 seconds using spinning-disk confocal microscopy. Movie frame rate: 20 frames/sec.
**Movie 2. Multicellular Ca\textsuperscript{2+} transients at the tissue level.**

An embryo expressing R-GECO1.0 was imaged during neural tube closure. Images show a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (seconds) is shown at the top left. Frames were captured every 20 seconds using spinning-disk confocal microscopy. Movie frame rate: 8 frames/sec.
**Movie 3. Effect of E-NTPDase1 on intracellular Ca^{2+} dynamics.**

Embryos expressing R-GECO1.0 without (left) and with E-NTPDase1 (right) were imaged during neural tube closure. Images show a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. The elapsed time (minutes: seconds) is shown at the top left. Frames were captured every 40 seconds using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.
Movie 4. Dynamics of F-actin and intracellular Ca$^{2+}$ in the neural plate.

An embryo expressing Lifeact-EGFP (left) and R-GECO1.0 (right) was imaged during neural tube closure. Images show a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (minutes: seconds) is shown at the top left. Frames were captured every 20 seconds using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.
Movie 5. Photolysis of NPE-caged IP$_3$ in the neural plate.

An embryo expressing EGFP-CAAX (left) and R-GECO1.0 (right) was imaged during neural tube closure. Imaging shows a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (seconds) is shown at the top left. A UV light was shone onto a central circular region for 120–125 seconds. Frames were captured every 5 seconds using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.

An embryo expressing EGFP-CAAX (left) and R-GECO1.0 (right) in control ringer solution was imaged during neural tube closure. Imaging shows a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (minutes: seconds) is shown at the top left. A UV light was shone onto a central circular region for 10–30 seconds. Frames were captured every 1 second using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.
Movie 7. Effect of photolysis of DMNPE-caged ATP on the neural plate.

An embryo expressing EGFP-CAAX (left) and R-GECO1.0 (right) in DMNPE-caged ATP-containing ringer solution was imaged during the neural tube closure. Imaging shows a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Elapsed time (minutes: seconds) is shown at the top left. A UV light was illuminated to a central circular region for 10–30 seconds. Frames were captured every 1 second using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.
Movie 8. The effect of photolysis of DMNPE-caged ATP on the neural plate of an embryo injected with 5mis-N-cadherin-Mo.

A control-Mo-injected embryo expressing EGFP-CAAX (left) and R-GECO1.0 (right) in DMNPE-caged ATP-containing ringer solution was imaged during neural tube closure. Imaging shows a dorsal view of the presumptive anterior spinal cord region; anterior is to the top. The elapsed time (minutes: seconds) is shown at the top left. A UV light was shone onto a central circular region for 10–30 seconds. Frames were captured every 1 second using spinning-disk confocal microscopy. Movie frame rate: 15 frames/sec.

An N-cadherin-Mo-injected embryo expressing EGFP-CAAX (left) and R-GECO1.0 (right) in DMNPE-caged ATP-containing ringer solution was imaged during the neural tube closure. Dorsal view of the presumptive anterior spinal cord region; anterior is to the top. Number in the left top indicates time (minutes: seconds). UV light was shone onto a central circular region for 10–30 seconds. Frames were captured every 1 second using spinning-disk confocal microscopy and the movie plays at 15 frames/sec.
Movie 10. Single and combined effects of Ca^{2+} transients (pulse) and constrictive nature of apical cell surface (Acn) on the modeled epithelial tissue.

Cells outlined in bold are in an active state. The simulation time is shown at the top left; simulation conditions are indicated below each tissue. Frames were captured every 20 simulation times. Movie frame rate: 20 frames/sec.
Movie 11. Collectivity effect of the Ca$^{2+}$ transient (pulse) on the modeled epithelial tissue

Cells outlined in bold are in an active state. The simulation time is shown at the top left. The number of active periods is indicated below each tissue. Frames were captured every 20 simulation times. Movie frame rate: 20 frames/sec.